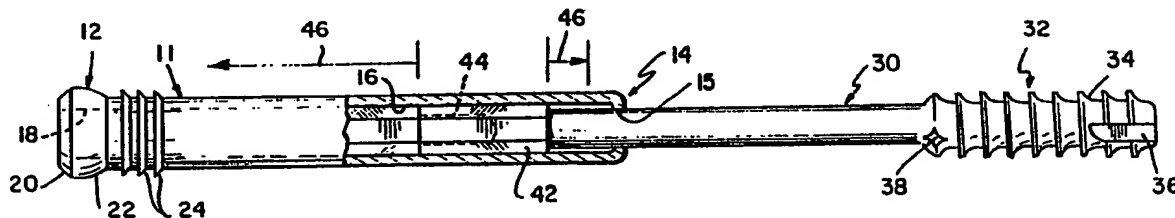




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**(54) Title: VARIABLE LENGTH FIXATION DEVICE**



**(57) Abstract**

A variable length fixation device (10) for insertion into a hole formed in two or more bone fragments has a barrel portion (11) and a fastener element (30). The barrel portion (11) is secured to an inside surface of the hole in a proximal one of the bone fragments. The fastener element (30) is telescopically mounted to the barrel portion (11) and is extendable into a distal one of the bone fragments. The assembly prevents lateral movements of the distal fragment, relative to the proximal fragment, while allowing axial relative movements (i.e., linear movements along the longitudinal axis of the fastener element) to occur. In a preferred embodiment, the fastener element (30) is a cannulated bone screw having a hex-shaped cross-section (42) on one end which is telescopically received into a hex-shaped interior (16) of the hollow barrel portion (11). The two components are preferably permanently joined to form a one-piece assembly having a variable overall length. The fixation device of the present invention is substantially insertable in its entirety into the hole which extends across the fracture site, and may be installed with a minimal amount of trauma and damage to surrounding bone and soft tissues.

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Variable Length Fixation Device

This invention relates generally to orthopedic fixation devices and, more particularly, to a variable length fixation device which is especially well-suited  
5 for fixation of fractures of the femoral neck, tibial plateau and pelvis.

Fractures of the type which commonly occur in the femoral neck, tibial plateau and pelvis require internal fixation for proper and timely healing. Such  
10 fixation is normally accomplished with nails or lag screws which hold the fractured pieces of bone together along the fracture site until healing is complete.

One known technique for fixation of fractures of the above types is the so-called Asnis Guided Screw  
15 System presently marketed by Howmedica, Inc., of New York, N.Y., and partially described in U.S. Patents 4,383,527 and 4,450,835. The Asnis system utilizes one or more rigid lag screws which are installed across a fracture site over guide pins to rigidly secure the  
20 bone fragments in close proximity to one another. In treating a fracture of the femoral neck, for example, three or four screws are inserted through the lateral cortex of the femur, and extend across the fracture site and into the subchondral region of the femoral  
25 head. Each screw must be carefully selected for the exact size because they are "fixed length screws."

The rigid screws of the Asnis system may provide

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relatively good initial fixation of the fracture. However, during the post-operative period, resorption of bone on either side of the fracture line may occur. In this event, a fracture which has been fixed with  
5 rigid screws may no longer be firmly compressed or impacted along the fracture line. The rigid screws assume the primary load bearing function, and physiological compression which might otherwise occur at the fracture site is prevented. Alternatively, the  
10 screws may "slide" in the holes drilled in the femur as resorption occurs, and the heads of the screws will be forced outwardly away from the femur and into the surrounding soft tissues, i.e., the heads become "extruded." Under these conditions, an extended period  
15 may be required for complete and proper healing of the fracture, or the extrusion of the screws may result in loss of the fracture fixation and/or subsequent loss of the fracture reduction which may result in the fracture failing to unite which is otherwise known as a  
20 non-union.

Use of the Asnis system requires proper selection of screw size (i.e., length) to fit a particular fracture and bone size. An inventory of twenty screw sizes with lengths ranging from 35 mm to 130 mm in 5 mm  
25 increments is recommended.

Other known devices for fixation of fractures of the femoral neck are illustrated and described in U.S.

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Patents 2,612,159; 2,702,543 and 4,438,762. These devices typically depend on a side plate (often referred to as a trochanteric plate in the above-referenced patents) which has a shank portion and a tubular guide sleeve which form an angle with each other of approximately 135 degrees. The shank portion is provided with a number of holes and is positioned along the lateral cortex of the femur below the area of the fracture. A plurality of bone screws extend through the holes in the shank and into the shaft of the femur to hold the plate in position. The tubular guide sleeve extends into a hole which has been drilled or reamed into the femur, and which extends along the center line of the femoral neck. A single lag screw or nail extends through the guide sleeve, across the fracture site and into the femoral head. The nail or screw is free to move telescopically within the guide sleeve so that contact between the bone fragments is maintained, notwithstanding the occurrence of resorption at the fracture site. The tubular guide sleeve of the plate, which is firmly attached to the shank of the femur, provides lateral support for the nail or screw and, at least in some cases, is designed to prevent relative rotation between the bone fragment attached to the nail or screw and the shank of the femur.

Use of a fixation device which incorporates a side

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plate requires the insertion of additional holes and screws into the shaft of the femur, which may already be weakened by the original injury, or by osteopathic disease. The installation and removal of these devices  
5 require relatively large incisions and a relatively complex surgical procedure. The recovery period during which the patient must be at least partially immobilized is increased, along with the probabilities of occurrence of infections and other complications.

10 An object of the present invention is to provide a fixation device which is simple to install and to remove, and which may be installed and removed with a minimal amount of trauma and damage to surrounding tissues.

15 Another object of the present invention is to provide a fixation device having a variable length which may be versatily used in a number of fracture types and situations. A major practical advantage is one of cost since two of these screws can greatly  
20 reduce the number of device sizes which must be maintained in inventory.

Yet another object of the present invention is to provide a fixation device which avoids or minimizes other problems associated with prior art devices, while  
25 offering advantageous features to both surgeon and

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patient in the treatment of many types of fractures.

These and other objects of the invention are attained in a variable length fixation device for insertion into an opening formed in one or more bone fragments which comprises a barrel portion, means for  
5 securing the barrel portion to an interior surface of the opening in the bone fragments, and a fastener element. The fastener element is telescopically mounted to the barrel portion and extends into a distal  
10 one of the bone fragments for preventing lateral movements of the distal fragment relative to the barrel portion and a proximal one of the fragments. The opening in the bone fragments extends along a line which is substantially transverse to a plane of  
15 fracture between the fragments, and the telescopically mounted fastener means allows axial relative movements (i.e., movements parallel to the longitudinal axis of the fastener) of the fragments along the transverse line of the opening.

20 In a preferred embodiment, the means for securing the barrel portion to the interior surface of the opening comprises a plurality of locking rings formed on an outer surface of the barrel portion. The locking rings interact with a surface of the opening in the  
25 proximal bone fragment to prevent axial movements

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(i.e., migration into or out of the opening) of the barrel portion subsequent to insertion of the device. The fastener element preferably comprises a screw portion having a plurality of threads on a first end thereof for fastening to the distal bone fragment, and having means on a second end thereof for slidably mounting the screw portion to the barrel portion. In an especially preferred embodiment, the screw portion has a hexagonally-shaped cross-section and outer surface. In this embodiment, the barrel portion is hollow and has a hexagonally-shaped inner surface. The hexagonally-shaped outer surface of the screw portion is slidably mounted within the hollow barrel portion in an adjacent and mating relationship to the hexagonally-shaped inner surface, such that the screw portion is rotationally fixed relative to the barrel portion.

A preferred embodiment of the present invention includes means for detachably connecting a wrench to the barrel portion to allow the barrel portion to be rotated which automatically advances the screw portion into the distal fragment. This means is preferably a hexagonally-shaped recess in a proximal end of the barrel portion. In a preferred embodiment of the invention, the barrel portion and the fastener element are cannulated (i.e., hollow) and are adapted for



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insertion over a guid pin positioned along the transverse line of the opening. The barrel portion and fastener element are preferably permanently assembled to form a unitary fixation device.

5       An especially preferred embodiment of the invention is termed a Variable Length Compression (VLC<sup>TM</sup>) bone screw assembly which comprises a barrel portion and a screw portion. The barrel portion is provided with means for securing the barrel portion to an interior  
10 surface of the opening in the proximal fragment to prevent axial movements of the barrel portion subsequent to insertion. The screw portion has a first end which is provided with means for fastening the screw portion to the distal bone fragment, and a second  
15 end which is mounted to the barrel portion. The screw portion is axially movable, but rotationally fixed, relative to the barrel portion and is preferably cannulated (i.e., hollow). In this preferred embodiment, the barrel portion is hollow and the second  
20 end of the screw portion is telescopically mounted within the barrel portion. The second end of the screw portion has a hexagonal cross-section, and an internal shape of the hollow barrel portion has a matching hexagonal cross-section such that, when the two  
25 hexagonal cross-sections are placed together in mating

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relationship with each other, relative rotation of the barrel portion and screw portion is prevented. The cannulated screw portion is further provided with threads on at least a portion of an internal surface to provide a means for connecting the screw portion to a compression tool. In the preferred embodiment of the invention, the means for fastening the first end of the screw portion to the distal bone fragment comprise a plurality of cancellous screw threads. Self-cutting flutes are provided on either end of the threads for easing insertion into and extraction from the distal bone fragment. The barrel portion and the screw portion are preferably permanently assembled by a swaging technique to form the complete bone screw assembly.

A preferred method of installing the bone screw assembly of the present invention includes a first step of placing a guide pin across the fracture site to define the desired location for placement of the bone screw assembly. A cannulated reamer is used to widen at least an outer portion of the hole to accommodate the barrel of the bone screw assembly. If desired or required, the remaining portion of the hole may be tapped to reduce the effort required for insertion of the screw portion into relatively dense bone tissue.

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After the hole has been reamed and, in some cases, tapped, the bone screw assembly is inserted into the hole, and a tool is used to turn the barrel portion, causing the barrel portion to twist the screw portion  
5 into the bone fragment. The screw portion is advanced under fluoroscopic control until the desired level of penetration has been achieved. After the required number of bone screw assemblies have been installed, the fracture may be compressed or impacted, as desired.

10 The design of the bone screw assembly of the present invention permits physiological compression at the fracture site during the post-operative period, notwithstanding the possible occurrence of resorption of bone tissue along the fracture. Accordingly, firm  
15 fixation is dynamically maintained throughout the period of fracture healing. Other advantages include ease of installation and removal, reduced trauma to surrounding bone and soft tissues, greater versatility resulting from the variable length feature, and reduced  
20 cost for inventory requirements.

Other objects, advantages and novel features of the present invention will become apparent from the following detailed description of the invention, when considered in conjunction with the accompanying  
25 drawings.

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BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 shows a side view of the barrel portion of a preferred embodiment of the variable length fixation device of the present invention.

Figure 2 shows a side view of the screw portion of a preferred embodiment of the variable length fixation device of the present invention.

Figure 3 shows a side view of a preferred embodiment of the variable length fixation device of the present invention.

Figures 4-11 illustrate the steps of a preferred method of using the preferred embodiment of Figure 3 in treating a fracture of the femoral neck.

DETAILED DESCRIPTION OF THE DRAWINGS

A preferred embodiment of the present invention is shown in Figures 1, 2 and 3. This preferred embodiment is designated a Variable Length Compression Screw, or a VLC<sup>TM</sup> Screw. The complete bone screw assembly (10) is shown in Figure 3. Bone screw assembly 10 comprises two main component parts which are separately illustrated in Figures 1 and 2, and which are discussed in detail below.

Figure 1 shows a side view of barrel portion 11 of

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the present invention. Barrel portion 11 is a generally elongate hollow structure having a head portion 12 on a first end thereof. The opposite end 14 of barrel portion 11 is open to receive the screw portion (30 in Figure 2) of bone screw assembly 10, as described in detail below. Inner surface 16 of barrel portion 11 is hex-shaped throughout at least a portion (and preferably the entire length) of barrel portion 11. Hex-shaped interior surface 16 extends all the way through head portion 12 or, alternatively, a hex-shaped recess 18 is provided in the end of head portion 12 to receive a detachable tool or wrench which is used to rotate barrel portion 11 and, in the preferred embodiment, the rest of bone assembly 10. Outer surfaces 20 and 22 of head portion 12 are spherical in shape, such that the overall shape of head portion 12 is that which would result from the intersection of portions of two spherical bodies. As illustrated in Figure 1, the overall diameter of the widest point of head portion 12 (i.e., the intersection of spherical surfaces 20 and 22) is only slightly larger than the diameter of the remaining portions of barrel portion 11. Barrel portion 11 is further provided with three equally spaced locking rings 24 immediately adjacent head portion 12. As will be explained below, locking

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rings 24 are intended to prevent outward migration of barrel portion 11 after placement of bone assembly 10 within a hole formed in a bone.

Figure 2 shows screw portion 30 of bone screw assembly 10. Screw portion 30 has a first end 32 which is provided with a plurality of threads 34 for fastening screw portion 30 to bone tissue. A plurality of cutting flutes 36 are provided on the outer end of threads 34 to ease the process of inserting or  
10 threading screw portion 30 into bone tissue. Cutting flutes 38 are also provided on the opposite end of threads 34 to ease the process of extracting bone screw assembly 10 after healing of the fracture is complete.

A second end 40 of screw portion 30 preferably has  
15 a hexagonally-shaped outer surface 42 which extends axially along at least a portion of the outer surface of screw portion 30. Hex-shaped outer surface 42 is intended to mate with hex-shaped inner surface 16 of barrel portion 11, such that when the two portions 11  
20 and 30 are joined, relative axial rotation between the two is prevented. The mating relationship between surfaces 16 and 42 is such that axial relative movement between portions 11 and 30 is uninhibited. Screw portion 30 is cannulated (i.e., hollow) and a portion  
25 of the inner surface of screw portion 30 is provided

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with threads 44 for purposes of compressing a fracture ,  
as will be described in additional detail below.

Figure 3 shows a side view of bone screw assembly  
10 after barrel portion 11 and screw portion 30 have  
5 been joined. Barrel portion 11 and screw portion 30  
are preferably permanently joined by swaging end  
portion 14 of barrel portion 11 to form an inwardly  
extending lip 15 around the circumference of end  
portion 14, subsequent to insertion of screw portion 30  
10 within barrel portion 11, to prevent subsequent  
disassembly. As discussed, mating hex-shaped surfaces  
16 and 42 prevent relative rotational movement between  
portions 11 and 30. However, as illustrated by arrow  
46, relative axial movements between portions 11 and 30  
15 are uninhibited.

Figures 4-11 illustrate a preferred method of using  
bone screw assembly 10. As previously noted, bone  
screw assembly 10 is especially well-suited for  
fixation of fractures occurring in the femoral neck,  
20 the tibial plateau, and pelvis. For purposes of  
illustration, Figures 4-11 describe the use of bone  
screw assembly 10 for fixation of a fracture of the  
femoral neck.

After the fracture has been reduced and the femur  
25 exposed, guide pin 50 is introduced through the lateral

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cortex of the femur. Guide pin 50 will be used to ensure proper lateral placement of bone screw assembly 10. Two additional guide pins 52 and 54 are placed below guide pin 50 in spaced apart relation and in parallel to guide pin 50 to form a preferred triangular configuration. The triangular configuration of holes 50', 52' and 54', each of which accept a corresponding guide pin, is shown in Figure 6. Each pin extends through the lateral cortex and across the fracture site into an acceptable position and depth in the femoral head. All guide pins and screw assemblies are preferable kept at or above the level of the lesser trochanter (indicated by dotted line 56 in Figures 5 and 6) to prevent the possible creation of stress risers which might jeopardize the integrity of the femoral shaft at the subtrochanteric level.

With reference to Figure 7, a direct measurement gauge 60 is used to determine the correct VLC<sup>TM</sup> screw size. An advantage to the present invention is that the variable length feature of bone screw assembly 10 allows for a drastic reduction in the required number of screw sizes. At present, two screw sizes are contemplated. The first will range from 59 mm to 76 mm (2-5/16" to 3"), and the second will range from 76 mm to 110 mm (3" to 4-5/16").



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Following measurement to determine proper screw size, a cannulated reamer 62 is placed over the guide pins to form three parallel holes in the proximal bone fragment (i.e., the femur) which will receive barrel portion 11 of bone screw assembly 10 (see Figure 8). Each hole is drilled along a line which extends generally transversely to a plane which extends, in a generally coplanar relationship, across the fracture site in the femoral neck. A groove 64 on the body of reamer 62 indicates proper depth for reaming. Reaming beyond the depth indicated by groove 64 may cause unnecessary bone loss and prevent proper screw fixation. As illustrated in Figure 9, a cannulated bone tap 66 may be used over the guide pins when hard, dense bone is encountered in the femoral head. Alternatively, screw portion 30 may be threaded directly into the distal bone fragment (i.e., the femoral head) without tapping or reaming this portion in advance.

After the guide pins have been placed and measured, and after the holes have been reamed and (if desired) tapped, bone screw assembly 10 is inserted into each of the holes (see Figure 10). A T-shaped hex wrench 68 is used to rotate barrel portion 11 and, consequently, screw portion 30 into position over the guide pin.

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When wrench 68 is pushed and rotated in a clockwise direction, threads 34 of screw portion 30 will engage the bone tissue and screw portion 30 will telescopically advance out of barrel portion 11 along the guide pin. Screw portion 30 is advanced under fluoroscopic control to the subchondral level of the joint, or until desired placement is achieved. After a screw assembly has been placed in each of the three holes, locking rings 24 on the barrel of each assembly are seated into the lateral cortex by tapping on the handle of wrench 68 (see Figure 11) which drives the rings into the cortex. The rings serve to prevent the barrel from backing out of the upper femoral shaft.

After the bone screw assemblies are in place, the fracture may be compressed or impacted, as preferred. For fractures of the pelvis, tibial plateau and femoral neck in younger patients, where osteopenia infrequently occurs, a compression tool 70 may be used to compress the fracture. A compression rod extends through the hollow barrel portion 11 of the screw assembly and is threaded into internal threads 44 of screw portion 30. The compression rod is then placed in tension, while barrel portion 11 is held in place, to draw the bone fragments together by drawing screw portion 30 into barrel portion 11 to firmly compress the fracture.

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This is especially valuable for bringing together the two major fragments of bone in femoral neck fractures, tibial plateau fractures, and pelvic fractures. Alternatively, an impaction tool (72 in Figure 11) may  
5 be placed against the femur in the area immediately adjacent the bone screw assemblies, and firm impaction of the fracture can be achieved by tapping on the end of the impaction tool. Impaction tool 72 preferably has recessed holes 74 which are placed over the heads  
10 of the bone screw assemblies to allow the impaction forces to be equally distributed on the lateral cortex of the femur around the screws.

Although the present invention has been described and illustrated by reference to a particularly  
15 preferred embodiment (i.e., the VLC<sup>TM</sup> bone screw assembly), other types of fixation devices may advantageously incorporate the features of the present invention. In its broadest sense, the present invention is intended to encompass such devices (for  
20 example, a variable length nail). Furthermore, although the fixation device of the present invention is shown and discussed with reference to a particular type of fracture, and although the specific embodiment shown is particularly well-suited for treating certain  
25 types of fractures, use of the invention is not limited

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to these applications.

From the preceding description of the preferred  
embodiments, it is evident that the objects of the  
invention are attained. Although the invention has  
5 been described and illustrated in detail, it is to be  
clearly understood that the same is intended by way of  
illustration and example only and is not to be taken by  
way of limitation. The spirit and scope of the  
invention are to be limited only by the terms of the  
10 appended claims.

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Claims

1. A variable length fixation device for insertion into an opening formed in at least a proximal one of two or more bone fragments, along a line which  
5 is substantially transverse to a plane of a fracture between the fragments, comprising:

a barrel portion, insertable into the opening in the proximal fragment;

means for securing the barrel portion to an  
10 interior surface of the opening in the proximal fragment to prevent axial movements of the barrel portion subsequent to insertion; and

fastener means, telescopically mounted to the barrel portion and extendable into a distal one of  
15 the two or more bone fragments, for preventing lateral movements of the distal fragment, relative to the proximal fragment, while allowing axial relative movements of said fragments along the transverse line of the opening.

20

2. A variable length fixation device according to Claim 1, wherein said means for securing the barrel portion to the interior surface of the opening comprises a plurality of locking rings formed on an  
25 outer surface of the barrel portion.

3. A variable length fixation device according to

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Claim 1, wherein said fastener means comprises a screw portion having a plurality of threads on a first end thereof for fastening to the distal bone fragment, and having means on a second end thereof for slidably mounting the screw portion to the barrel portion.

4. A variable length fixation device according to Claim 3, wherein the second end of said screw portion has a hexagonally-shaped outer surface, and wherein said barrel portion is hollow and has a hexagonally-shaped inner surface, and wherein the hexagonally-shaped outer surface of the screw portion is slidably mounted within the hollow barrel portion in adjacent and mating relation to the hexagonally-shaped inner surface, such that the screw portion is rotationally fixed relative to the barrel portion.

5. A variable length fixation device according to Claim 4, further comprising means for detachably connecting a wrench means to the barrel portion to allow the barrel portion to be rotated to advance the screw portion into the distal fragment.

6. A variable length fixation device according to Claim 5, wherein said means for connecting a wrench means comprises a hexagonally-shaped recess in a proximal end of the barrel portion.

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7. A variable length fixation device according to Claim 1, wherein said barrel portion and said fastener means are hollow and are adapted for insertion over a  
5 guide pin positioned along the transverse line of the opening.

8. A variable length fixation device according to Claim 1, wherein said barrel portion and said fastener  
10 means are permanently assembled to form a unitary fixation device.

9. A variable length compression bone screw assembly for insertion into an opening formed in at  
15 least a proximal one of two or more bone fragments, comprising:

a barrel portion insertable into the opening in the proximal fragment;

means for securing the barrel portion to an  
20 interior surface of the opening in the proximal fragment to prevent axial movements of the barrel portion subsequent to insertion;

a screw portion having first and second ends, and having means on said first end for fastening  
25 the screw portion to the distal bone fragment; and

means for mounting the second end of the screw portion to the barrel portion such that the screw

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portion is axially movable and rotationally fixed,  
relative to the barrel portion.

10. A variable length compression bone screw  
5 assembly according to Claim 9, wherein said barrel  
portion is hollow, and wherein the second end of the  
screw portion is telescopically mounted within the  
hollow barrel portion.

10 11. A variable length compression bone screw  
assembly according to Claim 10, wherein at least a  
portion of the second end of the screw portion has a  
hexagonal cross-sectional shape, and wherein an  
internal surface of the hollow barrel portion has a  
15 matching hexagonal shape.

12. A variable length compression bone screw  
assembly according to Claim 9, wherein said means for  
securing the barrel portion to the interior surface of  
20 the opening comprises a plurality of locking rings  
formed on an outer surface of the barrel portion.

13. A variable length compression bone screw  
assembly according to Claim 9, wherein said screw  
25 portion is hollow and wherein at least a portion of an



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internal surface of the screw portion is threaded.

14. A variable length compression bone screw assembly according to Claim 9, wherein said means on  
5 said first end of the screw portion for fastening the screw portion to the distal bone fragment comprises a plurality of threads.

15 15. A variable length compression bone screw assembly according to Claim 14, wherein said threads  
10 include at least one self-cutting flute on either end thereof, for easing insertion into and extraction from the distal bone fragment.

15 16. A variable length compression bone screw assembly according to Claim 9, wherein the barrel  
portion and the screw portion are permanently assembled  
to form the bone screw assembly.

20

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## AMENDED CLAIMS

[received by the International Bureau on 27 June 1989 (27.06.89)  
original claims 1-16 amended; new claims 17-22 added (8 pages)]

1. A variable length fixation device for insertion into an opening formed in at least a proximal one of two or more bone fragments, along a line which is substantially transverse to a plane of a fracture between the fragments, comprising:

a barrel portion, insertable into the opening in the proximal fragment;

means for securing the barrel portion to an interior surface of the opening in the proximal fragment to prevent axial movements of the barrel portion subsequent to insertion; and

fastener means, telescopically mounted to the barrel portion and extendable into a distal one of the two or more bone fragments, for preventing lateral movements of the distal fragment, relative to the proximal fragment, while allowing axial relative movements of said fragments along the opening;

wherein said fixation device has a variable overall length which is equal to the combined lengths of said barrel portion and said fastener means, and which is always greater than the length of said fastener means.

2. A variable length fixation device according to Claim 1, wherein said means for securing the barrel portion to the interior surface of the opening comprises a plurality of locking rings formed on an outer surface of the barrel portion.

3. A variable length fixation device according to Claim 1, wherein said fastener means comprises a screw portion having a plurality of threads on a first end thereof for fastening to the distal bone fragment, and having means on a second end thereof for slidably mounting the screw portion to the barrel portion.

4. A variable length fixation device according to Claim 3, wherein the second end of said screw portion has a hexagonally-shaped outer surface, and wherein said barrel portion is hollow and has a hexagonally-shaped inner surface, and wherein the hexagonally-shaped outer surface of the screw portion is slidably mounted within the hollow barrel portion in adjacent and mating relation to the hexagonally-shaped inner surface, such that the screw portion is rotationally fixed relative to the barrel portion.

5. A variable length fixation device according to Claim 4, further comprising means for detachably connecting a wrench means to the barrel portion to allow the barrel portion to be rotated to advance the screw portion into the distal fragment.

6. A variable length fixation device according to Claim 5, wherein said means for connecting a wrench means comprises a hexagonally-shaped recess in a proximal end of the barrel portion.

7. A variable length fixation device according to Claim 1, wherein said barrel portion and said fastener means are hollow and are adapted for insertion over a guide pin positioned along the transverse line of the opening.

8. A variable length fixation device according to Claim 1, wherein said barrel portion and said fastener means are permanently assembled to form a unitary fixation device.

9. A variable length compression bone screw assembly for insertion into an opening formed in at least a proximal one of two or more bone fragments, comprising:

a barrel portion insertable into the opening in the proximal fragment;

means for securing the barrel portion to an interior surface of the opening in the proximal fragment to prevent axial movements of the barrel portion subsequent to insertion;

a screw portion having first and second ends, and having means on said first end for fastening the screw portion to the distal bone fragment; and

means for mounting the second end of the screw portion to the barrel portion such that the screw portion is axially movable and rotationally fixed, relative to the barrel portion, such that an overall length of the bone screw assembly is defined by the combined length of the barrel portion and the screw portion, and wherein said overall length is always greater than the length of the screw portion.

10. A variable length compression bone screw assembly according to Claim 9, wherein said barrel portion is hollow, and wherein the second end of the screw portion is telescopically mounted within the hollow barrel portion.

11. A variable length compression bone screw assembly according to Claim 10, wherein at least a portion of the second end of the screw portion has a hexagonal cross-sectional shape, and wherein an internal surface of the hollow barrel portion has a matching hexagonal shape.

12. A variable length compression bone screw assembly according to Claim 9, wherein said means for securing the barrel portion to the interior surface of the opening comprises a plurality of locking rings formed on an outer surface of the barrel portion.

13. A variable length compression bone screw assembly according to Claim 9, wherein said screw portion is hollow and wherein at least a portion of an internal surface of the screw portion is threaded.

14. A variable length compression bone screw assembly according to Claim 9, wherein said means on said first end of the screw portion for fastening the screw portion to the distal bone fragment comprises a plurality of threads.

15. A variable length compression bone screw assembly according to Claim 14, wherein said threads include at least one self-cutting flute on either end thereof, for easing insertion into and extraction from the distal bone fragment.

16. A variable length compression bone screw assembly according to Claim 9, wherein the barrel portion and the screw portion are permanently assembled to form the bone screw assembly.

17. A variable length fixation device according to Claim 1, wherein said first length is approximately 59 mm., and wherein said second length is approximately 76 mm., and wherein said overall length is variably adjustable to intermediate lengths therebetween.

18. A variable length fixation device according to Claim 1, wherein said first length is approximately 76 mm, and wherein said second length is approximately 110 mm, and wherein said overall length is variably adjustable to intermediate lengths therebetween.

19. A variable length compression bone screw assembly according to Claim 9, wherein said first overall length is approximately 59 mm, and wherein said second overall length is approximately 76 mm, and wherein the overall length of the bone screw assembly is variably adjustable therebetween.

20. A variable length compression bone screw assembly according to Claim 9, wherein said first overall length is approximately 76 mm, and wherein said second overall length is approximately 110 mm, and wherein the overall length of the bone screw assembly is variably adjustable therebetween.



21. A variable length fixation device according to Claim 1, further comprising means for rotating the barrel portion, and wherein the fastener means is rotationally fixed, but axially movable, relative to the barrel portion, so that rotation of the barrel portion results in rotation of the fastener means so that the fastener means may be advanced into the distal bone fragment by rotating the barrel portion.

22. A variable length fixation device according to Claim 9, further comprising means for rotating the barrel portion, and wherein the screw portion is rotationally fixed, but axially movable, relative to the barrel portion, so that rotation of the barrel portion results in rotation of the screw portion so that the screw portion may be advanced into the distal bone fragment by rotating the barrel portion.

## STATEMENT UNDER ARTICLE 19

New Claims 1-16 correspond to original Claims 1-16, with amendments added to conform to the priority application pending before the U.S. Patent Office. New Claims 17-22 are additional dependent claims directed to particular features of preferred embodiments of the invention.

The above amendments have no impact on the description or the drawings in this application, and will not require any amendments or modifications to be made thereto.



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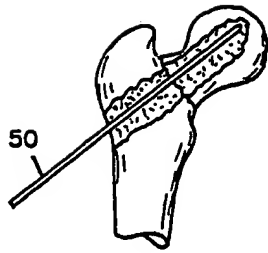


FIG. 4

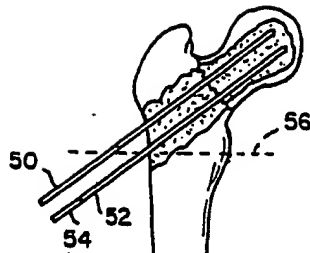


FIG. 5

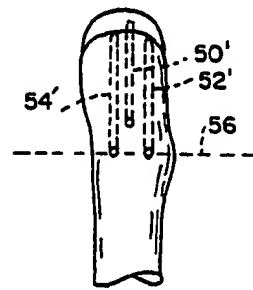


FIG. 6

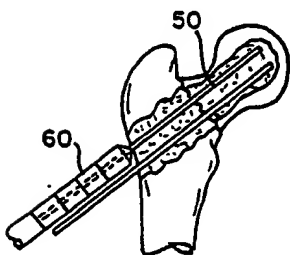


FIG. 7

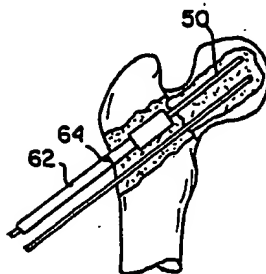


FIG. 8

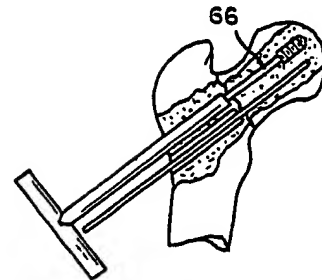


FIG. 9

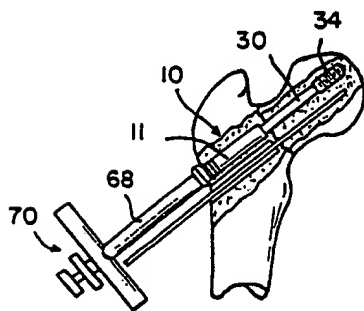


FIG. 10

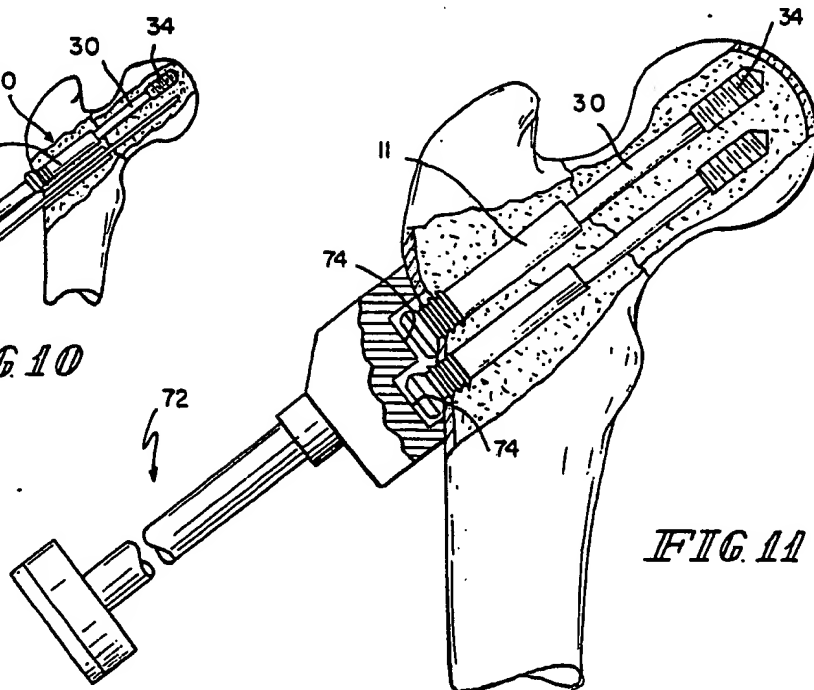


FIG. 11

SUBSTITUTE SHEET

# INTERNATIONAL SEARCH REPORT

PCT/US89/00430  
International Application No.

<b>I. CLASSIFICATION OF SUBJECT MATTER</b> (If several classification symbols apply, indicate all) <sup>6</sup>		
According to International Patent Classification (IPC) or to both National Classification and IPC		
IPC (4): A61 B 17/58 US. CL: 128/92YV		
<b>II. FIELDS SEARCHED</b>		
Minimum Documentation Searched <sup>7</sup>		
Classification System	Classification Symbols	
U.S.	128/92Y, 92YZ, 92YY, 92YK, 92YW, 92YV, 92YT 92YS, 92YP, 92YL, 92YF	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched <sup>8</sup>		
<b>III. DOCUMENTS CONSIDERED TO BE RELEVANT</b> <sup>9</sup>		
Category *	Citation of Document, <sup>11</sup> with indication, where appropriate, of the relevant passages <sup>12</sup>	Relevant to Claim No. <sup>13</sup>
A	US,A, 2,511,051 (DZUS) 13 June 1950. See entire reference.	
A	US,A, 2,682,265 (COLLISON) 29 June 1954. See entire reference.	
X	US,A, 3,051,169 GRATH) 28 August 1962. See entire reference.	1-3
A	US,A, 4,172,452 (FORTE ET AL) 30 October 1979. See entire reference.	
A	US,A, 4,441,492 (RYDELL ET AL) 10 April 1984. See entire reference.	
Y	US,A, 4,463,753 (GUSTILO) 07 August 1984. See entire reference.	6,15
Y	US,A, 4,628,923 (MEDOFF) 16 December 1986. See entire reference.	1-3,7,9, 10,12-14
A	US,A, 4,530,355 (GRIGGS) 23 July 1985. See entire reference.	
<p>* Special categories of cited documents: <sup>10</sup></p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art</p> <p>"&amp;" document member of the same patent family</p>		
<b>IV. CERTIFICATION</b>		
Date of the Actual Completion of the International Search		Date of Mailing of this International Search Report
28 March 1989		23 MAY 1989
International Searching Authority		Signature of Authorized Officer
US/PTO		Kevin G. Rooney

III. DOCUMENTS CONSIDERED TO BE RELEVANT (CONTINUED FROM THE SECOND SHEET)		
Category *	Citation of Document, with indication, where appropriate, of the relevant passages	Relevant to Claim No
Y	US,A, 4,640,271 (LOWER) 03 February 1987. See entire reference.	
Y	SU 1,007,659 (RUBL) 30 March 1983. See entire reference.	4,5,11
A	US,A 2,397,545 (HARDINGE) 02 April 1946. See entire reference.	
A	US,A, 2,612,159 (COLLISON) 30 September 1952. See entire reference.	
A	US,A, 2,702,543 (PUGH ET AL) 22 February 1955. See entire reference.	
A	US,A, 3,990,438 (PRITCHARD) 09 November 1976. See entire reference.	
A	US,A, 4,103,683 (NEUFELD) 01 August 1978. See entire reference.	
A	US,A, 4,341,206 (PERRETT ET AL) 27 July 1982. See entire reference.	
A	US,A, 4,381,770 (NEUFELD) 03 May 1983. See entire reference.	
Y	US,A, 4,438,762 (KYLE) 27 March 1984. See entire reference.	8,16
A	US,A, 4,450,835 (ASNIS ET AL) 29 May 1984. See entire reference.	
A	US,A, 4,641,640 (GRIGGS) 10 February 1987. See entire reference.	
A	US,A, 4,653,489 (TRONZO) 31 March 1987. See entire reference.	